



Quality assurance in radiotherapy

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Circuit of Radiotherapy

- Imaging
- Simulation
- Dosimetry

Irradiation

• Controls

- => CT, MRI, PET
- => Conventional, virtual
- => Calculations on TPS, Transfer (R & V)
- => Radiography, portal imaging or dosimetry in vivo
- => Accelerator or cobalt







The « risk » of treatment





Goal: <5% error



Sources of Error (uncertainty)



• imaging

- Density curve , position (irreproducible)...
- Simulation
 - Bad position (conformation, lasers) ...
- Dosimetry
 - Algorithm failed, Bad parameters, Bad configuration of TPS...
- Controls
 - Incorrect repositioning, error measures ...
- Irradiations
 - The problem of R & V, machine problems, bad irradiation (filter) ...





Sources of Error (uncertainty)



- Patient localization
- Organ motion
- Imaging (resolution, distortions,...)
- Definition of anatomy (outlines,...)
- Beam geometry
- Dose calculation
- Dose display and plan evaluation
- Plan implementation





Ensure different co-ordinate systems match...





The types of errors



• Random errors (one seance)

- Positioning
- Irradiation, location
- Systematic errors (all seances)
- Positioning, location
- Dosimetric Calculations
- Configuration of TPS, accelerator ...



All errors are human but the machines must be <u>reliable</u>





QUALITY as a goal

The totality of features or characteristics that bear on our ability to satisfy the stated or implied goal of effective patient care."

What is Quality Assurance?



"All those planned and systematic actions necessary to provide confidence that a product or service will satisfy given requirements for quality."

ISO 9000





QA and QC



Quality Assurance is the overall process which is supported by Quality Control activities



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Quality Control describes the actual mechanisms and procedures by which one can assure quality

Good QA systems in radiotherapy

✓ Improves work practices



✓ Would have prevented most of the major accidents

ISO 9000



QA systems









Part 1: Guidelines for selection and use

First published in Australia as AS 3900-1987/ISO 9000:1987.

- First published in New Zealand as NZS 5600.1:1987. AS 3900-1987/ISO 9000:1987 and NZS 5600.1:1987
- redesignated in 1990 and issued as Joint Nata Act redesignated in 1990 and issued as Joint Standard AS 3900—1987/NZS 9000:1990/ISO 9000:1987. Redesignated in 1992 as Joint Standard AS 3900.1—1987/NZS 9000:1990/ISO 9000:1987. Iointly revised and redesignated as Joint Standard AS/NZS 150 9000.1:1994.

- Many QA systems exist one important example is the ISO 9000 system
- They are highly successful in manufacturing industry because they do improve productivity and avoid costly mistakes



ISO 9000



- Comprehensive set of standards for QA (mainly in manufacturing and service industry)
- Adapted eg. by ESTRO to the radiotherapy environ
 - European Society for Therapeutic Radiology and Oncology (ESTRO) Advisory Report to the Commission of the European Union for the 'Europe Against Cancer Programme'. Quality Assurance in radiotherapy. Radiother. Oncol. 35: 61-73; 1995.





A Comprehensive QA Program typically comprises of

- Quality Assurance Committee
- Policies and Procedures Manual
- Quality Assurance team
- Quality audit
- Resources





QA Committee Membership



- Must represent the many disciplines within the department
- Should be chaired by the Head of Department
- As a minimum must include a medical doctor, a physicist, a radiotherapy technologist and an engineer responsible for service and maintenance
- Must be appointed and supported by senior management
- Must have sufficient depth of experience to understand the implications of the process
- Must have the authority and acces to the resources to instigate and carry out the QA process







Quality Assurance Committee





- Should be 'visible' AND accessible to staff
- Oversees the entire Quality Assurance program
- Writes policies to ensure the quality of patient care
- Assists staff in tailoring the program to meet the needs of the Department (using published reports as a guide)
- Monitor and audit the program to ensure that each component is being performed and documented





Policies and Procedures Manual



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- As a minimum, sections should exist for
 Administrative procedures
 - Clinical procedures
 - Treatment procedures
 - Physics procedures
 - Radiation safety





Continuous Quality Improvement



- CQI many other acronyms are available for this
 Dart of virtually all QA systems
- Part of virtually all QA systems
- Improved methods on cancer patient management are documented in clinical trial reports.
- Quality assurance protocols are continuously under development in many countries
- Regular Quality Assurance meeting for all members of a Section
- Continuing education lectures, workshops, journal clubs and must be available for all staff







Quality Assurance Program



Control of machines

- The imaging devices and the simulator
- Particles Accelerators
- Control of TPS and R&V
- Control of treatment (of patients)
 - Control of Positioning:
 - radiography and portal imaging
 - The cone beam CT
 - Control of dose
 - In vivo dosimetry
 - Pre-Treatment Controls





Imagers



- The simulator (-CT)
- The CT simulation







The simulator (-CT)





The simulator (CT)



Mechanical Control

- Table (Coach) Movements (Levels and security)
- Telemeter
- Diaphragms
- Scales of rotation
- Movements of the intensifier
- Anti-collision System
- Iso centric Verification
- Correspondence with light field and irradiated field
- Lasers





The simulator (-CT)



- Image Control
 - Graphic / fluoroscopy
 - Adapted Phantom
 - Spatial resolution
 - Distortion, focal spot size
- Dose Control
 - Measurement of parameters of low energy (50-130 kV) = > kV, mAs





The CT simulation





The CT simulation

AQUILAB



- Uniformity of Phantom
- Scale densities (dosimetry)











The Accelerators





The Accelerators



□ Internal control

- Daily CQMechanical and dosimetric
- Weekly CQ
 - Mechanical
- Monthly CQ
 - Mechanical and dosimetric
- Semestriel CQ
 - Mechanical and dosimetric
- Annual CQ
 - Mechanical and dosimetric
- **External Dose Control**





External Beam Radiotherapy Examples for daily QA



Safety

- door and other interlocks
- radiation warning lights (door, bunkers, equipment room)
- Verification of surveillance systems (camera + intercom)
- radiation area monitor



- Mechanical/optical "pointers"
- Radiation constancy check TOPS



PTW Linacheck





The TOPS



Every day, for all photon energies and at least one electron energy



	Not Applicable = N/A placed/Corrected = R/C Radiation Accuracy (Summary from d	ata forms)	of Weekly QA Checks From _// to// Linear Accelerator forms)						
	a. Photon High Energy MV	Baseline	Values:	Symmetry =	<u>"////////////////////////////////////</u>	Flatness	-	0%	
	i. Gantry Angle (°)					A latitess		_ 10	
	ii. Symmetry/Flatness (%)	1.1.1.1.1.1.1							
	III. Difference from Baseline (2%)								
	i. Gantry Angle (°)	Baseline	Values:	Symmetry =	%,	Flatness	=	_%	
	iii. Difference from Baseline (2%)	-	-						
	c. Electron Beams	One elect	tron ene	rgy per week					
	i. Electron Energy (MeV)								
	iii Gantry Angle (°)								
	iv. Symmetry/Flatness (%)	-							
	v. Difference from Baseline (2%)						_	-	
Example for weekly OA									
	Light/Radiation Field Coincidence	One gant	ry angle	per week	Section and				
Summary	a. Photon Energy (MV) b Cantry Angle (0°/180° 00° 270°)	_			_				
	c. Field Edges Difference (2 mm)		-	100.00				_	
	d. Field Centers Difference (2 mm)				0.000				
TTO C.	Safety System Functioning							_	
1.	Collision Avoidance (Touchguards)							- 1	
	Motion Enable (Deadman) Switch(es)								
	BEAM ON Light Above Door				1				
	Accessory Tray								
	a. Locking Mechanism (2 mm)								
	b. Tray Interlock								
	c. Tray Movement				1.1.1.6				
	Flattron Lockout in Photon Mode		_						
8.	Electron Beam Safety	One appl	icator pe	er week					
	a. Electron Cone (Number)							-	
	i. Cone Integrity		1-3	Marine and					
	II. Cone Code				_				
	A Photon Lockout Interlock								
	I. Photon Portal Film	-				1			
	e. Cone Touchguard								
From Constantinou 1992	Processor Sensitometry								
	Data						1		
	Physicist's/Technologist's Initials				-				
Comm	ients:								



weekly QA





weekly QA



• Checking the reference field size



Field size $20 \times 20 \text{ cm}$ SSD = 100 cm









Quality Assurance - Monthly



• Dosimetry

- Output constancy
- Backup monitors
- Central axis %DD constancy
- Flatness/symmetry constancy
- Timer end effect





Quality Assurance - Monthly



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- Safety interlocks
 - emergency
 - wedge etc
- Light/ radiation field coincidence
- Scales
- Isocentre position
- Cross hair position





Quality Assurance - Monthly



• Field size indicators



- Distance measuring indicators
- Jaw symmetry
- Latching of wedges, trays etc.



Wedge position (factors etc.)



Time requirements for QA



External beam per megavoltage unit

- daily: 30 minutes
- weekly: 2 hours
- monthly: > 4 hours
- annual: 2 days +







These are estimates only - a qualified expert must decide on the actual requirements for a particular treatment unit











Checking accessories (filters, door accessories, extension, ...)















Correspondence of the mechanical axis of the collimator with the axis of the beam

















• Check the dimensions of the radiation field



















Monthly Dosimetric (Beam performance) CQ



Using of the water phantom (with its software), ionization chambers, cable and electrometer:















• Ionisation chambers:











- PDD Acquisitions of photons :
 - Measuring conditions:



- SSD = 100 cm, normalization to the depth of maximum dose
- Field Size 10 x 10 cm
- All energy photons
- 0 to 25 cm depth











• Acquisitions profiles for uniformity and symmetry of photon fields:















Homogene

Non homogene



- - Transmission of filter :
 - Measure in the presence and absence of filter
 - tolerance <2% compared to the reference

- Standard

Motorise

Dynamique











PDD Acquisitions of electron:

- Conditions of Measurement:
 - SSD = 100 cm, normalisation à la profondeur du maximum de dose
 - SSD = 100 cm, normalization to the depth of maximum dose
 - Field Size 10 x 10 cm
 - Applicator 10 x 10 cm
 - All energy electrons
 - 0 to 25 cm depth











PDD Acquisitions of electron:







• Acquisitions profiles for uniformity and symmetry of photon fields:









CRITERIA FOR ACCEPTABILITY OF RADIOTHERAPY INSTALLATIONS

These criteria are valid for the normal clinical use of radiation therapy equipment and not (necessarily) for brachytherapy, intraoperative, dynamic, palliative and whole body radiation therapy equipment. In addition, radiation therapy treatment simulators are excluded from consideration. As indicated in the Introduction, the criteria presented may be used as remedial levels at which corrective action needs to be initiated. In a very few occasions, it might be justified to use the equipment clinically, even if the remedial level has been exceeded. Such a decision can only be taken after careful consideration of the responsible clinical physicist, with the knowledge of the clinicians and radiographers. For example, curative treatments demand a high stability of the treatment table height, especially during lateral irradiation. If due to mechanical tolerances the table height cannot be adjusted within the tolerance level, it still may be justified to perform palliative posterior anterior

or anterior-posterior treatments if no alternatives are present at all. The values given in Table 1 are based on recommendations in WHO (1988) and NCS (1995), with some modifications.

Test	remedial action level				
*Gantry rotation:	$\pm 1^{\circ}$				
*Yoke rotation:	$\pm 0,2^{\circ}$				
*Isocentre:	± 2 mm				
*Source distance indicators:	$\pm 2 \text{ mm}$				
*Beam axis indicators:	$\pm 2 \text{ mm}$				
*Numerical field indicators:	$\pm 2 \text{ mm}$				
*Light field indication:	$\pm 2 \text{ mm}$				
*Collimation system rotation:	$\pm 1^{\circ}$				
 Treatment couches: lateral and longitudinal scales vertical scales vertical deflection (with patient load) 	2 mm 2 mm 5 mm				
Treatment verification systems:manufacturer's specification(gantry angle, field size, collimator rotation, treatment time or monitor units, beam energy, etc.)					
*Immobilization devices	± 2 mm				
moulds, casts, breast bridges, head supports, arm or leg supports, bite-blocks, etc.)					
Patient alignment devices	± 2 mm				
Beam Performance and light- field accuracy					
*Light field indication (density measurements):	$\pm 1 \text{ mm per edge}$				
*Central axis dose calibration at reference position in phantom:	$\pm 3\%$ (photons) $\pm 4\%$ (electrons)				
Constancy chooks					

Test	remedial action level				
 X-ray beam beam flatness beam symmetry 	± 3% ± 3%				
Cobalt-60 and cesium-137 units - beam symmetry	± 3%				
Orthovoltage X-ray units - beam symmetry	± 6%				
Electron beamsflatness and symmetry	± 3%				
*Transmission factor of wedges and compensators	±2%				
 Dose monitoring system Precision Linearity dose rate effect Stability gantry angle 	$\begin{array}{c} \pm \ 0.5\% \\ \pm \ 1\% \\ \pm \ 2\% \\ \pm \ 2\% \\ \pm \ 3\% \end{array}$				
Treatment Planning System					
A computerized dose distribution can be considered as sufficiently accurate if calculated and measured doses differ by less than 2% at points of relevance for the treatment.					
– In regions involving very steep dose gradients, the observed position of a given					

isodose curve should differ from its calculated position by less than 0.3 cm.